

Innovative Integrated Instrumentation for Nanoscience





High Resolution Electronic Measurements in Nano-Bio Science

Differential measurements When, why and how

Giorgio Ferrari

Milano, June 2023

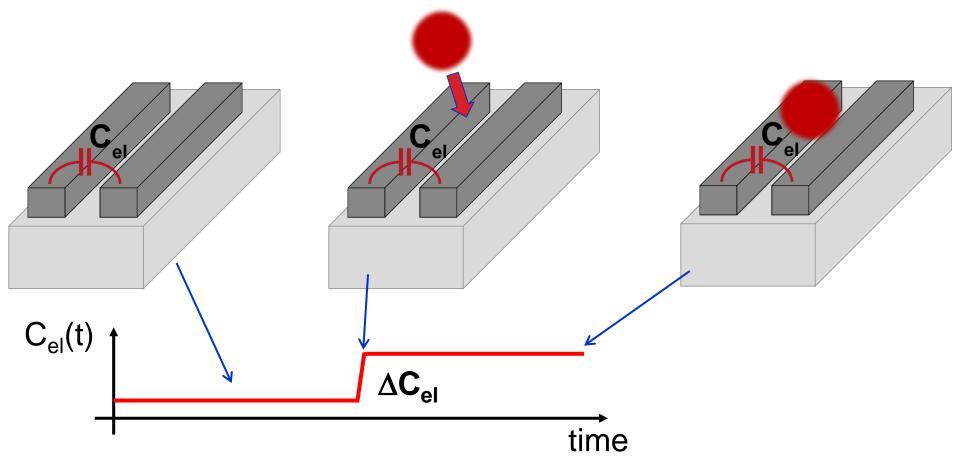
OUTLOOK of the LESSON

Motivation

- The differential approach
- Examples of implementation
- Limitations

Example: capacitive detection of particles

particle deposition on a surface (PM detector, cell monitor,...)



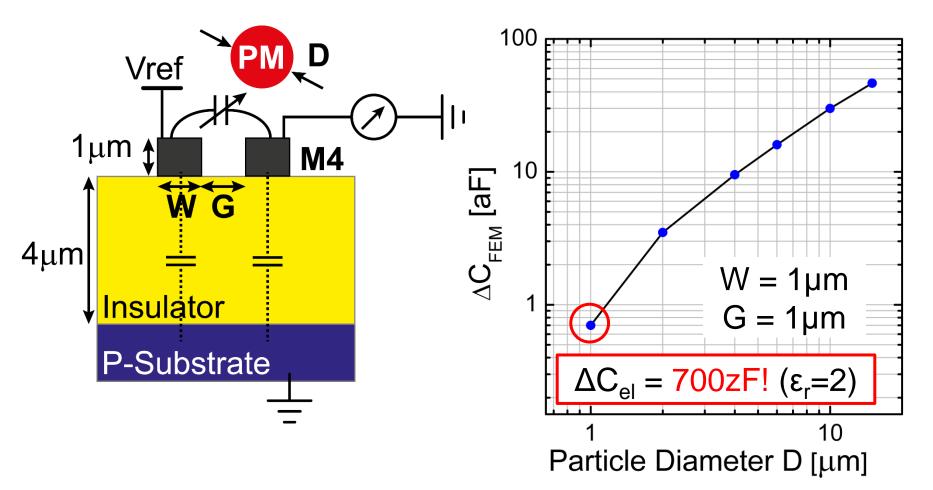
M. Carminati, Capacitive detection of micrometric airborne particulate matter for solid-state personal air quality monitors, *Sensors Actuators A* **219**, 2014.

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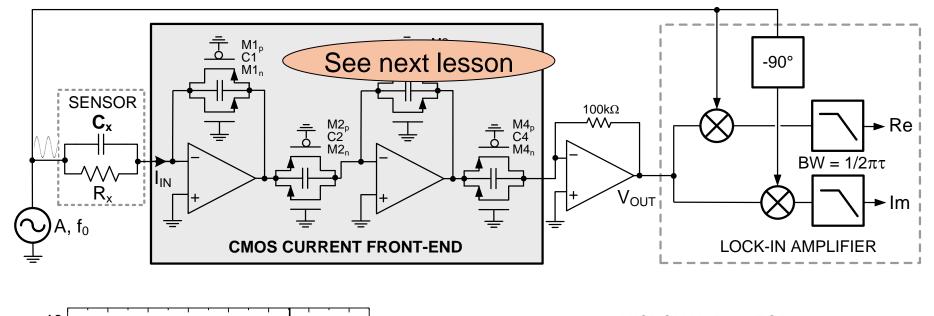
G. Ferrari – Differential measurements

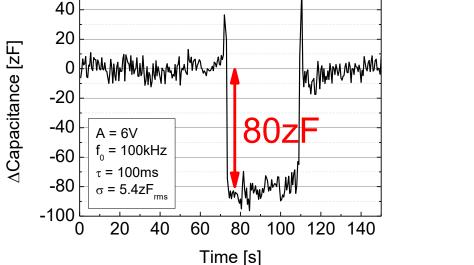
Electrodes Design

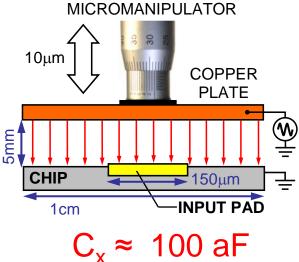
FEM Numerical Simulations



ZeptoFarad capacitance detection



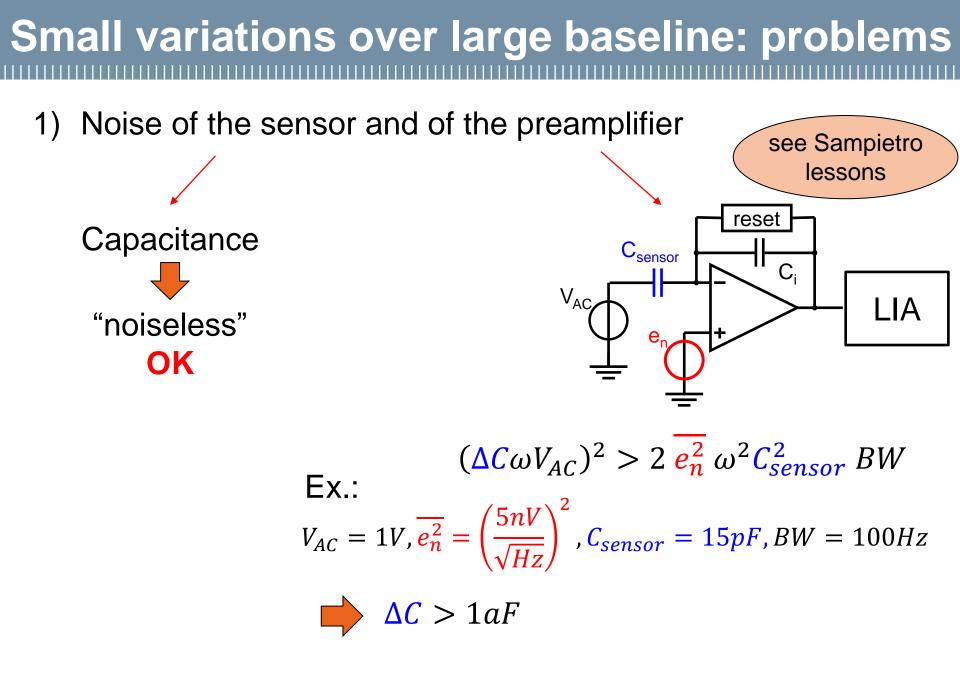




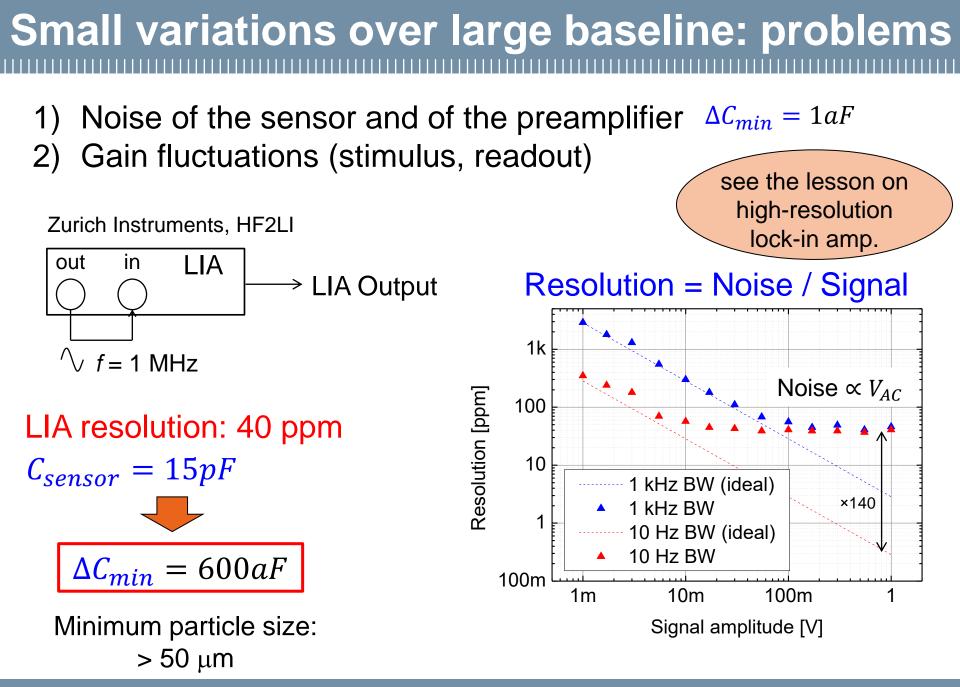
M. Carminati, G. Ferrari, F. Guagliardo, M. Sampietro, "ZeptoFarad capacitance detection with a miniaturized CMOS current front-end for nanoscale sensors", Sensors and Actuators A: Physical, Vol. 172, pp. 117-123 (2011)

Large sensitive area

Interdigitated electrodes: Example: area 1 mm² electrode gap 1 µm electrode length 500 μ m 1000 electrodes! Vref $C_{total} = 15 pF$ C_{stray} $\Delta C_{\text{target}} \approx 1 \text{ aF}$ for particle size of 1 µm 500 μm



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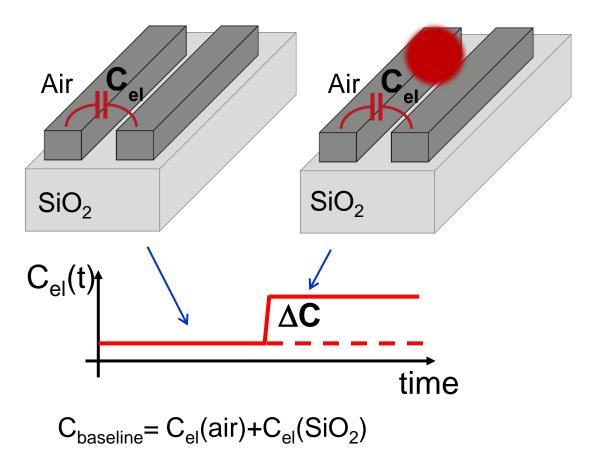


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G. Ferrari – Differential measurements

Small variations over large baseline: problems

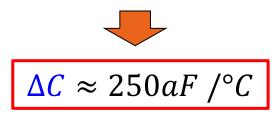
- 1) Noise of the sensor and of the preamplifier $\Delta C_{min} = 1 a F$
- 2) Gain fluctuations (stimulus, readout)
- 3) Baseline fluctuations



Temperature: $\Delta \epsilon_{air} \approx -2 \ ppm/^{\circ}C$ $\Delta \epsilon_{SiO_2} \approx 25 \ ppm/^{\circ}C$

 $\Delta C_{min} = 600 aF$

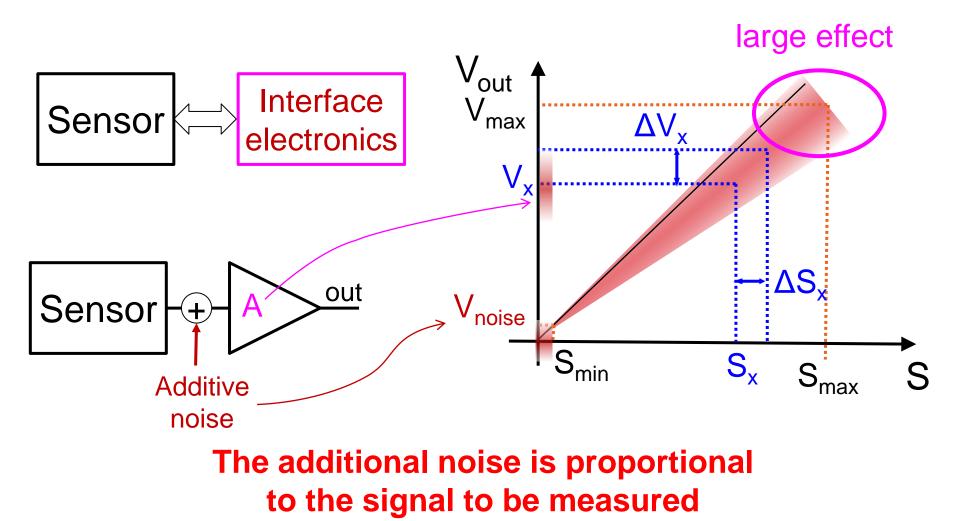
Humidity: $\Delta \epsilon_{air} \approx 1 \, ppm / \% RH$



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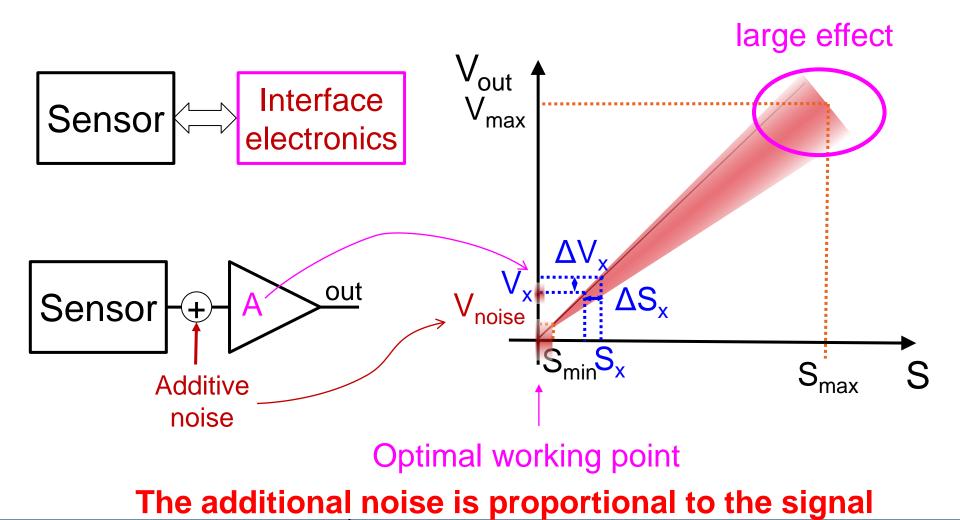
How to improve the resolution?

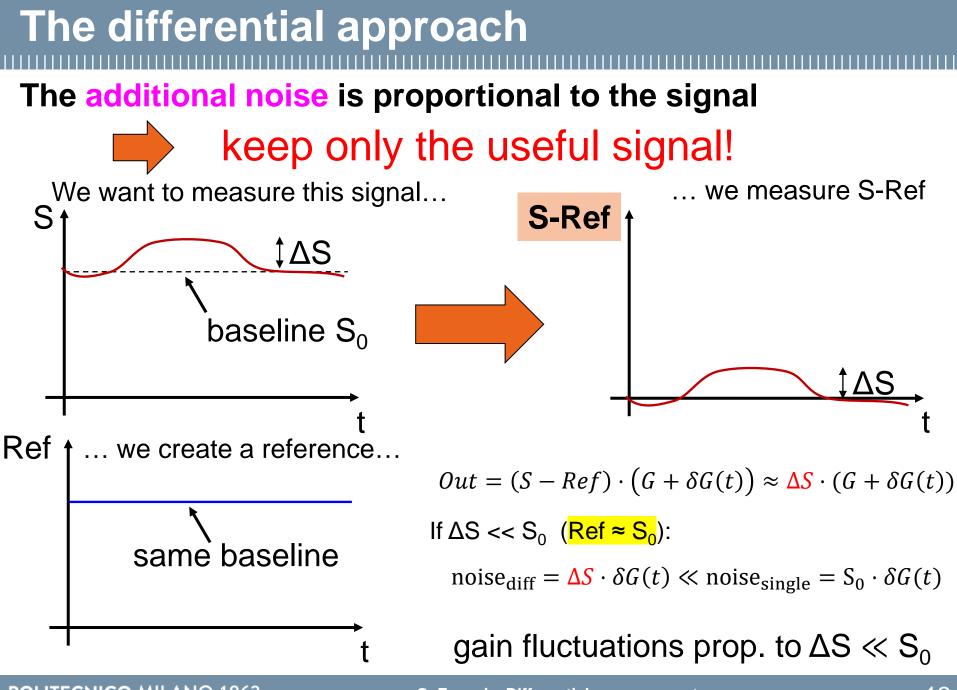
Slow measurements using good amplifiers and low noise sensors could be limited by gain fluctuations (DAC, amp., ADC)



How to improve the resolution?

Slow measurements using good amplifiers and low noise sensors could be limited by gain fluctuations (DAC, amp., ADC)

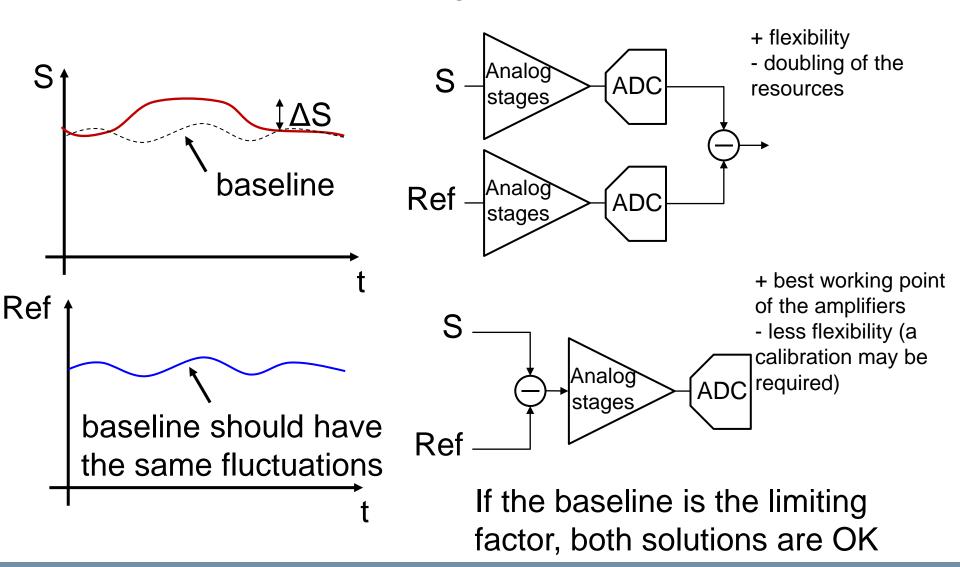




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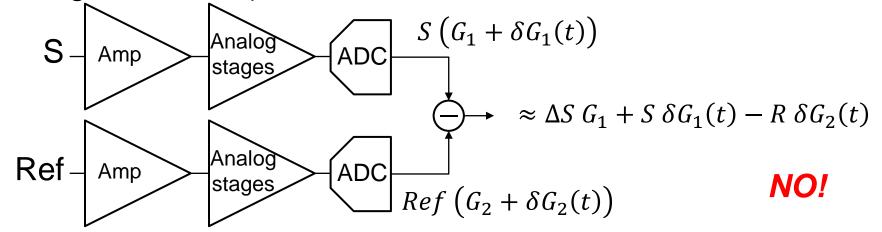
G. Ferrari – Differential measurements

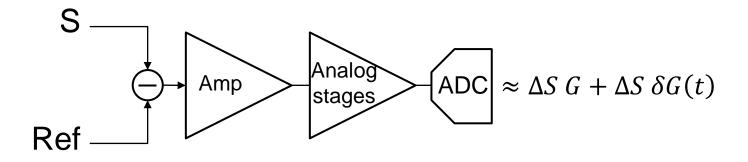
The differential approach: baseline fluctuations The Reference must share the gain fluctuations of the baseline:



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The differential approach: gain fluctuations If the limitation is set by the gain fluctuations of the acquisition chain the subtraction should be implemented as soon as possible (no digital domain!)

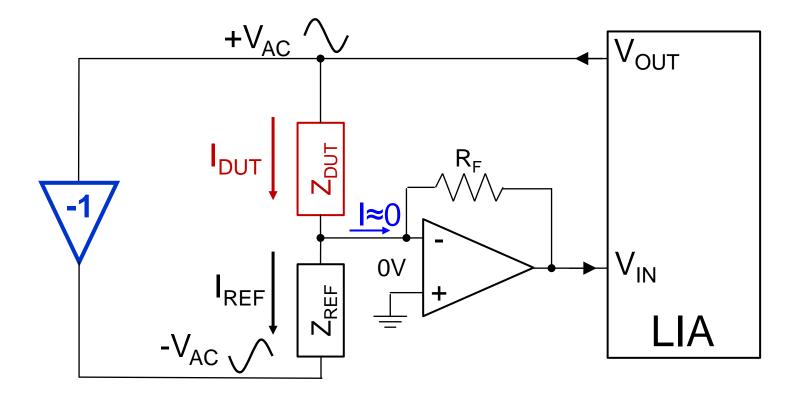




OUTLOOK of the LESSON

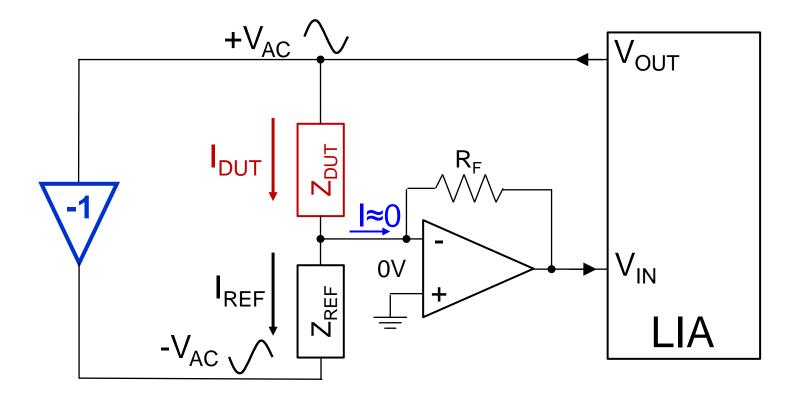
- Motivation
- The differential approach
- Examples of implementation
- Limitations

Differential current sensing



- Balanced structure: $Z_{REF} \approx Z_{DUT}$ \longrightarrow $I = V_{AC} \left(\frac{1}{Z_{DUT}} - \frac{1}{Z_{REF}} \right) = V_{AC} (Y_{DUT} - Y_{REF}) \approx 0$ \checkmark Less noise given by gain fluctuations (V_{AC}, R_F, ADC,...)
 - ✓ Amplifier optimization (gain, linearity, dynamic range)

Differential current sensing

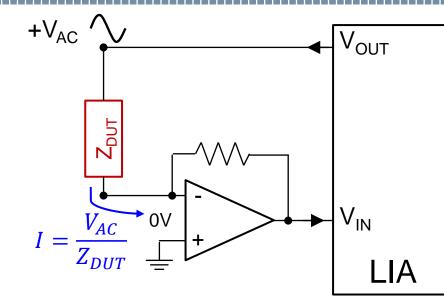


- Balanced structure: $Z_{REF} \approx Z_{DUT}$ $I = V_{AC} \left(\frac{1}{Z_{DUT}} - \frac{1}{Z_{REF}} \right) = V_{AC} (Y_{DUT} - Y_{REF}) \approx 0$
 - Z_{REF} adjacent to Z_{DUT} for sharing the same temp. fluctuations
 The inverting amplifier requires a stable gain!

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G. Ferrari – Differential measurements

Signal – reference matching: an example



Assuming:

- LIA resolution limit: 100ppm
- No other noise sources
- $Z_{\text{DUT}}(f_0) = 1M\Omega$

Goal:

• Detection of $\Delta Z_{DUT}(f_0)$ of 1Ω

Current variation

given by ΔZ_{DUT}

$$\begin{vmatrix} & \checkmark \\ |\Delta I| \approx \left| \frac{\partial I}{\partial Z_{DUT}} \Delta Z_{DUT} \right| = \left| \frac{V_{AC}}{Z_{DUT}^2} \Delta Z_{DUT} \right| = \left| I \frac{\Delta Z_{DUT}}{Z_{DUT}} \right|$$

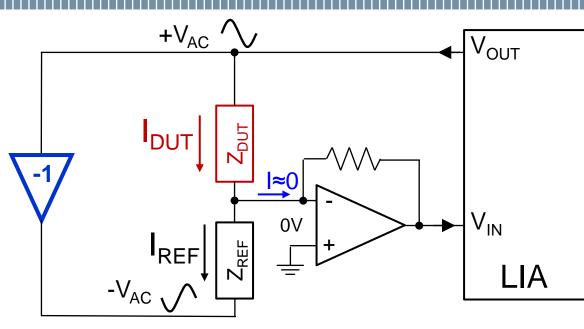
Minimum detectable impedance variation:

$$|\Delta I| > 10^{-4} I$$

$$\uparrow$$
100ppm
$$\Delta Z_{DUT} > 10^{-4} Z_{DUT} = 100\Omega$$

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Signal – reference matching: an example



Assuming:

- LIA resolution limit: 100ppm
- No other noise sources
- $Z_{DUT}(f_0) = 1M\Omega$

Goal:

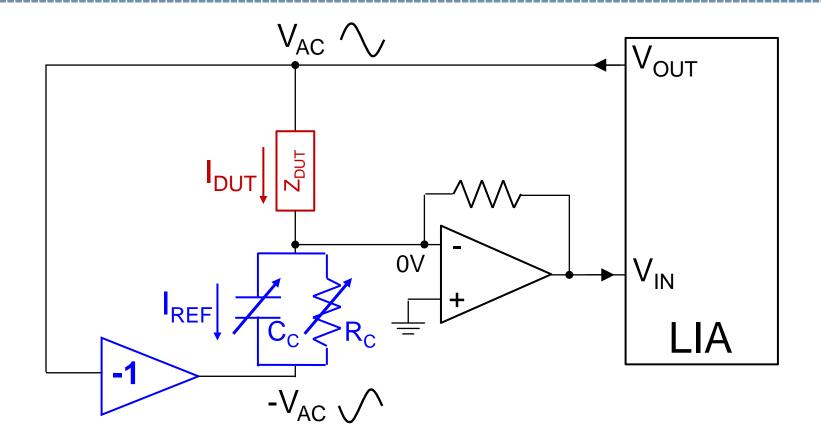
• Detection of $\Delta Z_{DUT}(f_0)$ of 1Ω

Current variation

given by
$$\Delta Z_{DUT}$$

 $|\Delta I| \approx \left| \frac{V_{AC}}{Z_{DUT}} \frac{\Delta Z_{DUT}}{Z_{DUT}} \right| > 10^{-4}I = 10^{-4} \left| \frac{V_{AC}}{Z_{DUT}} - \frac{V_{AC}}{Z_{REF}} \right|$
 $\left| \frac{\Delta Z_{DUT}}{Z_{DUT}} \right| > 10^{-4} \left| 1 - \frac{Z_{DUT}}{Z_{REF}} \right| \implies Z_{REF} \approx Z_{DUT} (1 \pm 1\%)$

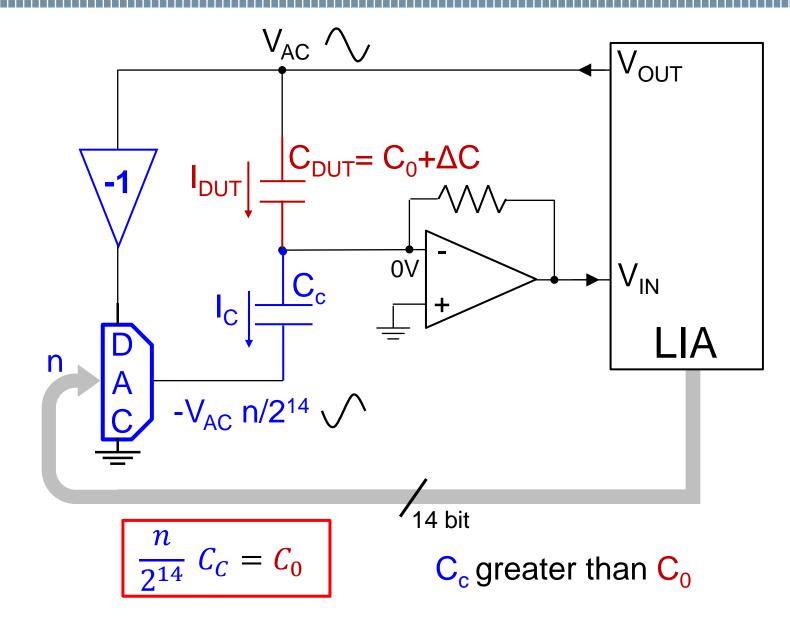
Calibration of the reference path



Calibration may be required to have I_{DUT}≈I_{REF} in *module and phase*

- 1) Manual setting of a capacitive trimmer C_c and resistive trimmer R_c
- 2) Digital setting of the reference path

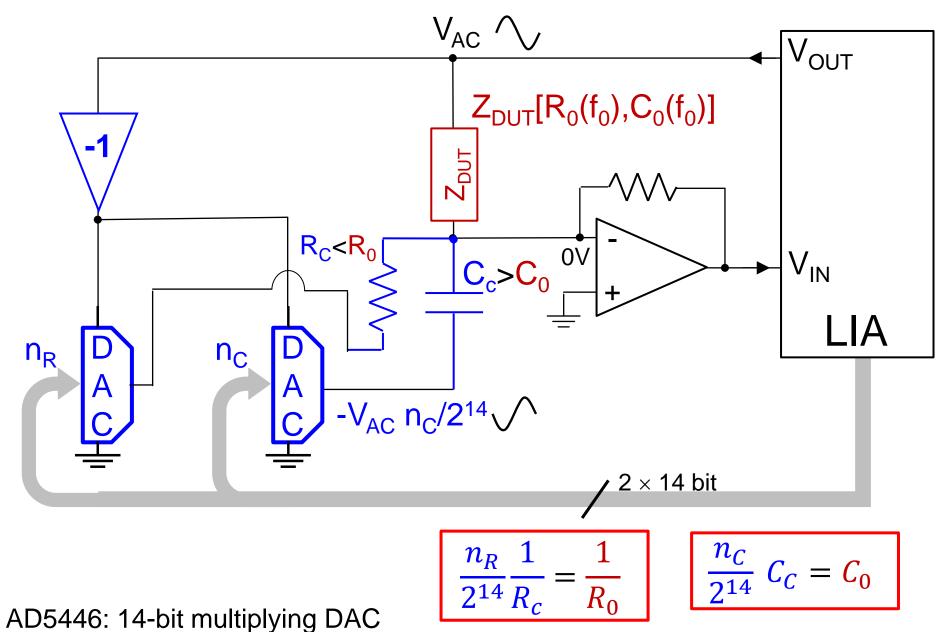
Digital control of the reference path



AD5446: 14-bit multiplying DAC, BW= 12MHz, gain temp. coef. <20 ppm /°C

Digital control of the reference path





Phase error

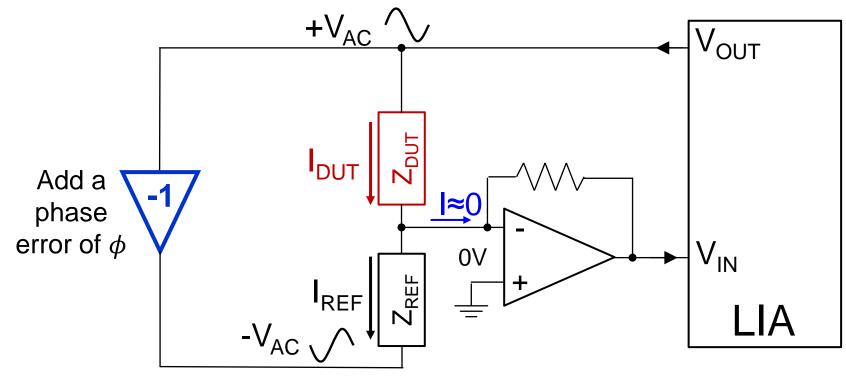
 $Im\{I(\omega)\}$

REF

DUT

error

Re{I(ω)}

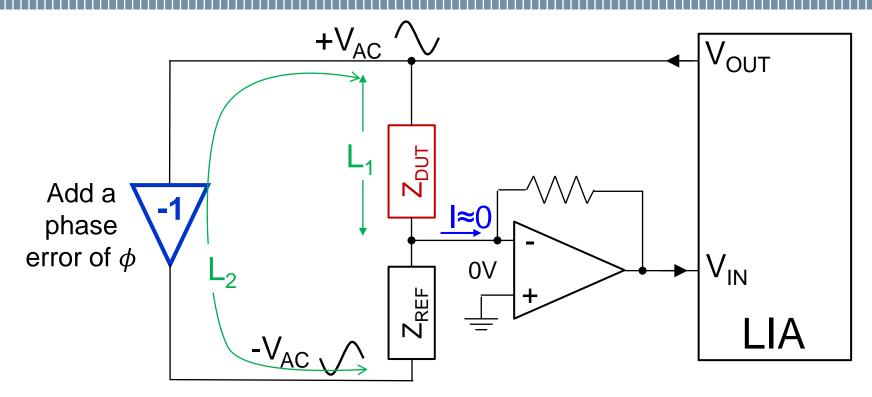


Assuming the ideal case of $Z_{REF} = Z_{DUT}$ we have a residual error:

$$V_{AC}\sin(\omega_0 t) - V_{AC}\sin(\omega_0 t + \phi) = -2 V_{AC}\sin\left(\frac{\phi}{2}\right)\cos\left(\omega_0 t + \frac{\phi}{2}\right)$$

It is an error in quadrature!

Phase error



Assuming the ideal case of $Z_{REF} = Z_{DUT}$ we have a residual error:

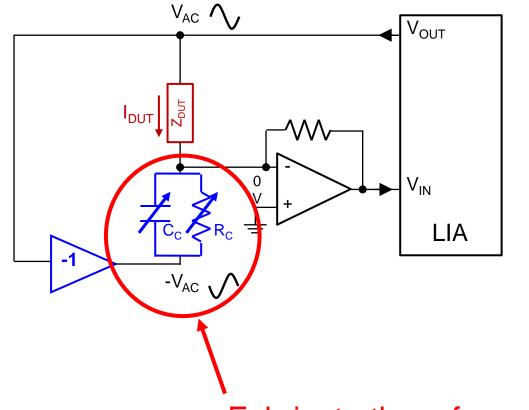
$$V_{AC}\sin(\omega_0 t) - V_{AC}\sin(\omega_0 t + \phi) = -2 V_{AC}\sin\left(\frac{\phi}{2}\right)\cos\left(\omega_0 t + \frac{\phi}{2}\right)$$

It is an error in quadrature!

For an error <1% $\rightarrow \phi$ < 0.6°

• BW >100· f_0 • If $f_0=10MHz \rightarrow connection length: |L_2-L_1| < 3.3cm 24$

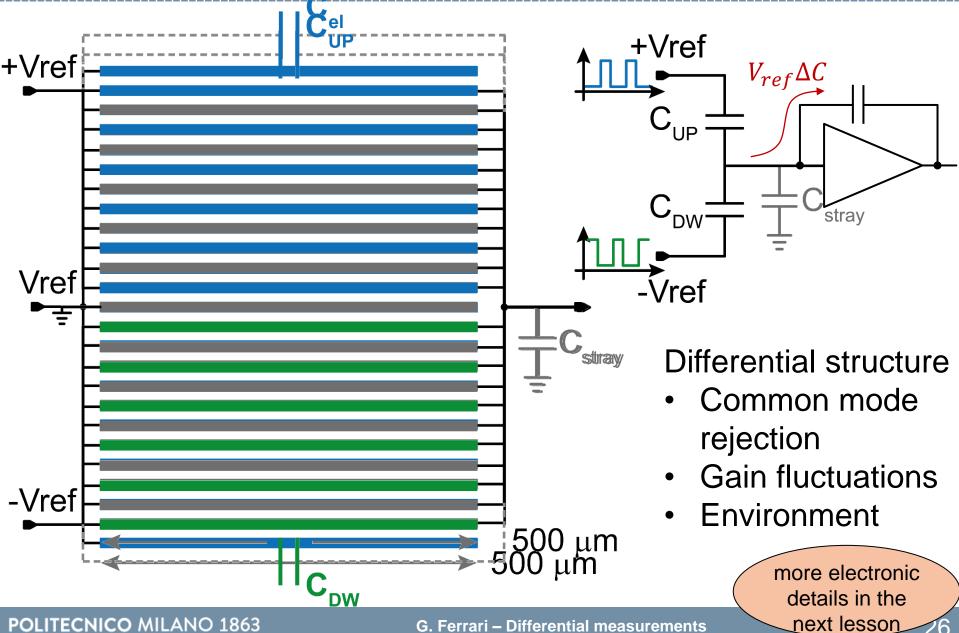
Generation of the reference path



- + general approach
- reduces the effect of gain fluctuations of the acquisition chain and the stimulus signal
- limited compensation for the environmental effects (temperature, humidity,...)
- long-term stability

Fabricate the reference path with the same technology as the DUT, if possible!

Differential electrodes architecture

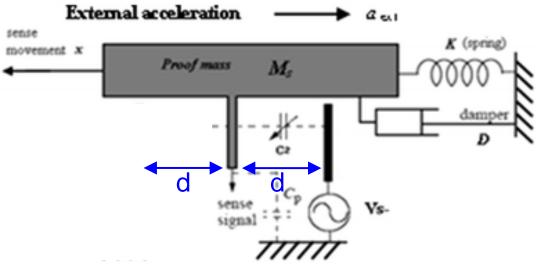


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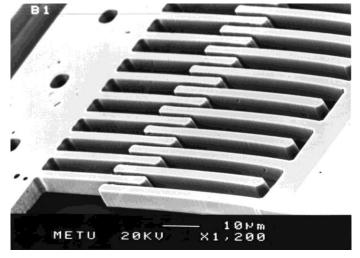
G. Ferrari – Differential measurements

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Design differential sensors if possible Example: MEMS capacitive sensors



<u>Microsystem Technologies, 2013,</u> pp 713–720, DOI: 10.1007/s00542-013-1741-z



http://www.microsystems.metu.edu.tr/gyroscope/ gyroscope.html

$$C_{1} = \epsilon \frac{A}{d + \Delta x} \cong C_{0} - \Delta C$$
$$C_{2} = \epsilon \frac{A}{d - \Delta x} \cong C_{0} + \Delta C$$

both arms of the differential structure are sensors

- Doubling the signal: C_2 - C_1 =2 ΔC
- Better linearity: compensation of even non-linearity
- Well-balanced structure
- Excellent rejection of common-mode interferences (temperature,...)

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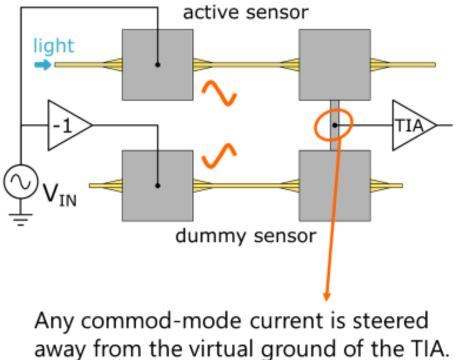
Dummy sensor

Differential sensor topology

Main CLIPP problems:

- The coupling between the electrodes generates a current much larger than the small variations to be measured.
- Sensitivity to temperature variations.
- Crosstalk between CLIPPs on different waveguides due to light in the oxide and substrate.





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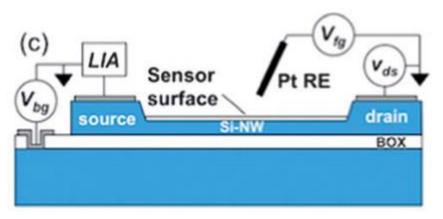
F. Zanetto – Transparent detection of light

F. Zanetto's lesson

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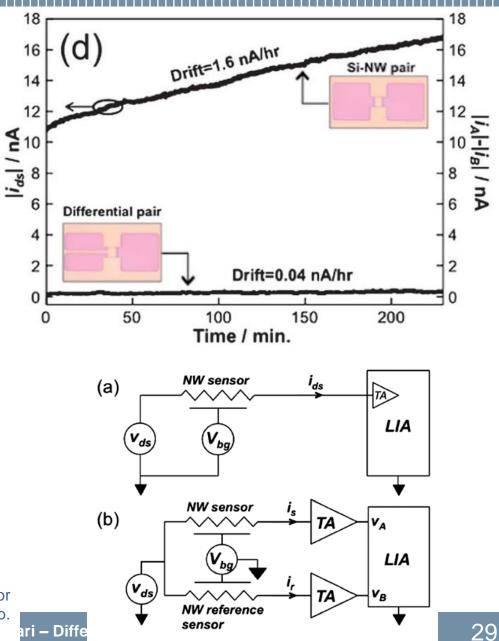
Differential biosensors

Ex.: silicon nanowire DNA sensor



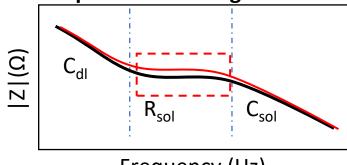
- AC measurement (LIA) for reducing the 1/f noise of the nanowire
- suffer from drift due to ion migration at the gate-oxide interface → differential meas.

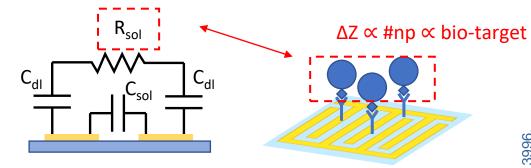
A. De, et al. "Integrated label-free silicon nanowire sensor arrays for (bio)chemical analysis," *Analyst*, vol. 138, no. 11, pp. 3221–3229, 2013, doi: 10.1039/c3an36586g.



Differential Impedance Biosensing

Impedance Sensing



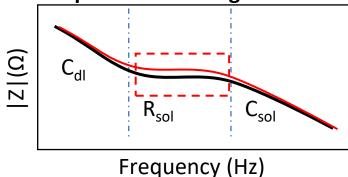


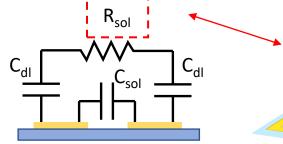
Frequency (Hz)

Resistance variation at the end of the experiment is related to the number of polystyrene NP's, i. e. to the specific nanosized biological target.

Differential Impedance Biosensing

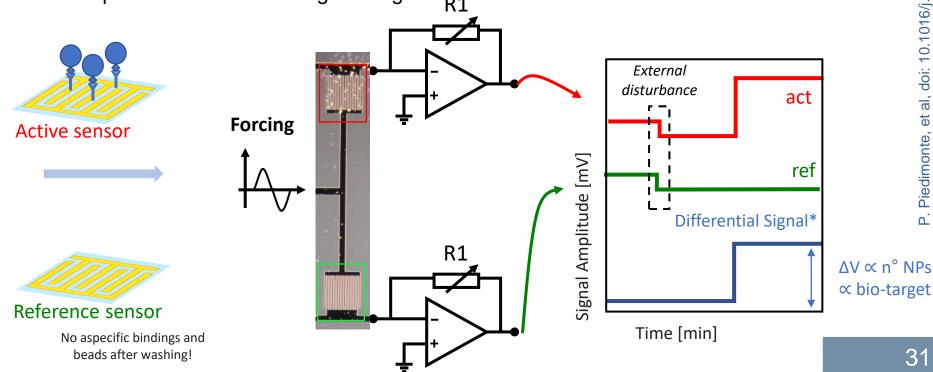
Impedance Sensing





 $\Delta Z \propto \#np \propto bio-target$

Resistance variation at the end of the experiment is related to the number of polystyrene NP's, i. e. to the specific nanosized biological target. **R1**



(A)

(B)

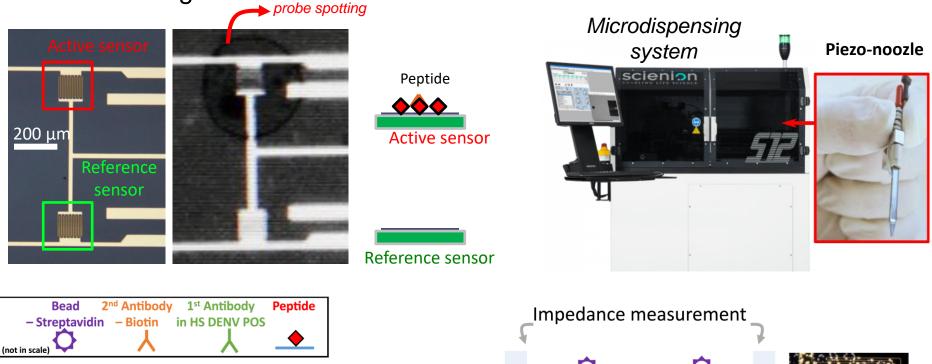
Biochip preparation

Local functionalization of the **active sensor** \rightarrow avoid non-specific binding

outside sensing area

Active sensor

Reference sensor

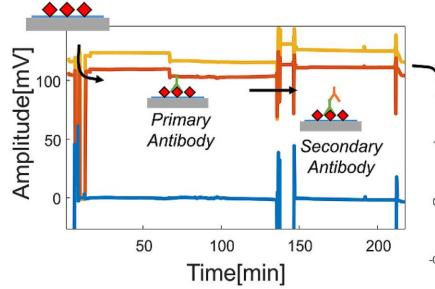


1. Incubation

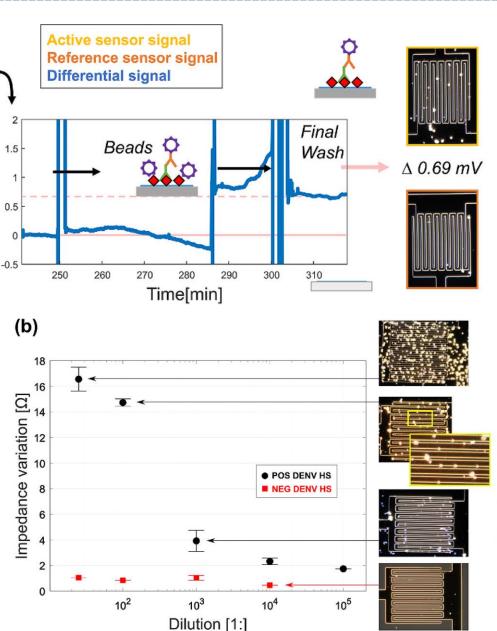
washing

2. Beads counting

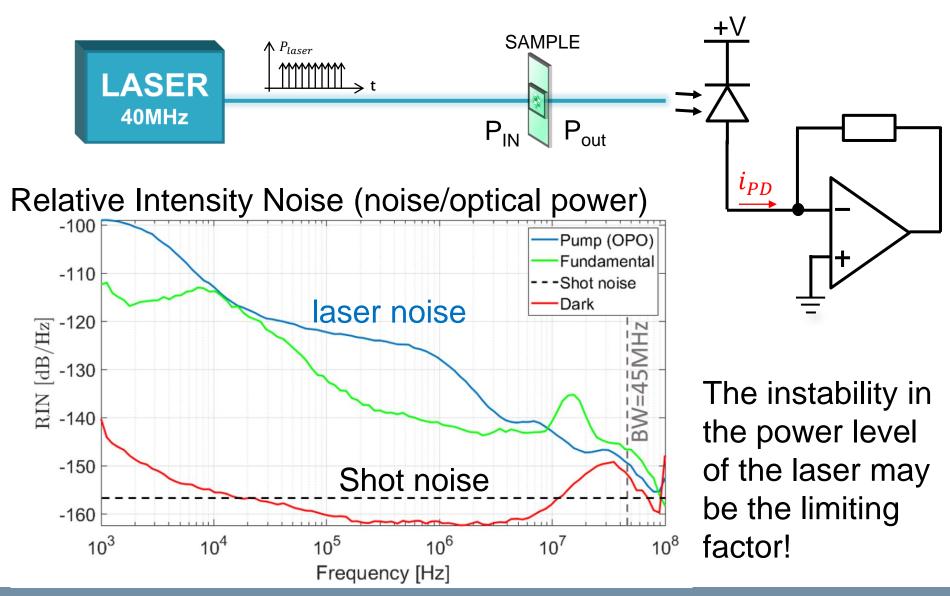
Results for Dengue Virus detection in human serum



- Human Serum samples positive to anti-DNV IgG antibodies
- Clinically relevant concentration
- Control: HS negative to anti-DENV IgG antibodies
- P. Piedimonte, et al, "Differential Impedance Sensing platform for high selectivity antibody detection down to few counts: A case study on Dengue Virus," Biosens. Bioelectron., vol. 202, p. 113996, Apr. 2022, doi: 10.1016/j.bios.2022.113996.



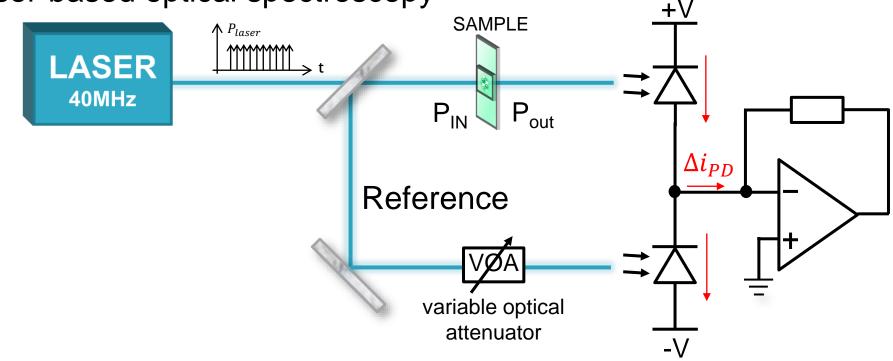
Laser-based optical spectroscopy



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Balanced optical detection

Laser-based optical spectroscopy

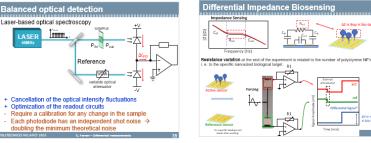


- + Cancellation of the optical intensity fluctuations
- + Optimization of the readout circuits
- Require a calibration for any change in the sample
- Each photodiode has an independent shot noise → doubling the minimum theoretical noise

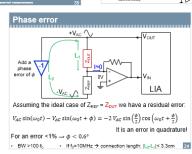
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Drawbacks of the differential approach

- While differential measurements offer several advantages, there are also some drawbacks to consider:
- Additional complexity for the generation of the reference path
- Calibration may be required for a well-matched structure
- Sensor response vs. frequency (spectroscopy) or temperature or bias,... could be difficult
- Increase the minimum theoretical noise



 Pay attention to the phase response and propagation delays



Summary

- A large baseline causes difficulties:
 - Gain fluctuations
 - Baseline fluctuations
 - Gain, linearity, and dynamic range of the acquisition chain
- Differential approach
 - Subtract the large baseline
 - Design a differential sensor if possible! (or use a dummy sensor)
 - A calibration may be required

• Alternative: ratiometric approach

